Sonographic Sleuthing: Techniques to Distinguish Pathology from Artifact

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Course Description

Have you ever paused during a scan and asked yourself, "Is that real—or just an artifact?" You're not alone. In this session, we'll explore the various types of sonographic artifacts—both helpful and problematic—and review techniques to tell them apart from true anatomical or pathological findings. We'll walk through practical ways to make that distinction using tools and settings already at your fingertips, like harmonics, compounding, focal zone placement, and Doppler adjustments. Through case examples and image comparisons, you'll pick up useful tips to fine-tune your scanning technique and feel more confident knowing what's real, and what's not.

Learning Objectives:

- Define and categorize common sonographic artifacts, identifying which are beneficial and which hinder diagnostic accuracy.
- Apply advanced image optimization techniques, including spatial compounding, harmonic imaging, and focal zone adjustment, to enhance diagnostic image quality.
- Differentiate true pathology from artifact using sonographic reasoning and pattern recognition in both grayscale and Doppler imaging.
- Evaluate the clinical significance of accurate artifact identification and discuss its impact on diagnostic confidence and patient outcomes.



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Artifact Foundations – Physics Meets Pattern Recognition

What Are Artifacts?

- Artifacts are image features that do not accurately represent the anatomy or reflectors being scanned.
- They may appear as echoes that are misplaced, distorted, falsely enhanced, or entirely fictitious.
- Artifacts can be diagnostic (useful), nondiagnostic, or confounding (misleading).
- Artifact categories we will discuss include: Grayscale Artifacts, Doppler Artifacts, and Equipment-Related Artifacts.





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Attenuation-Based Artifacts

- **Posterior shadowing** occurs behind high-attenuation structures (e.g., bone, stones).
- Acoustic enhancement is seen posterior to low-attenuation structures (e.g., cysts, bladder).
- Artifacts result from varying tissue attenuation rates compared to surrounding tissue.
- Useful for diagnosis: Shadow = solid/dense; Enhancement = cystic/fluid-filled.

Acoustic Enhancement

- Acoustic enhancement appears as increased echogenicity posterior to low attenuators (i.e., fluid-filled structures).
- It is also known as through transmission or posterior enhancement.
- Commonly seen behind cysts, bladder, vessels, etc.
- This artifact can **confirm the cystic nature** of a lesion and guide diagnostic decisions.



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Acoustic Shadowing

- Occurs when sound waves are strongly attenuated by dense structures such as bone, stones, or air.
- Results in a hypoechoic or anechoic band posterior to the object.
- Clean shadowing (sharp and dark) typically indicates bone or calculus.
- Dirty shadowing (diffuse and noisy) suggests air-containing structures.





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Edge Shadow Artifact

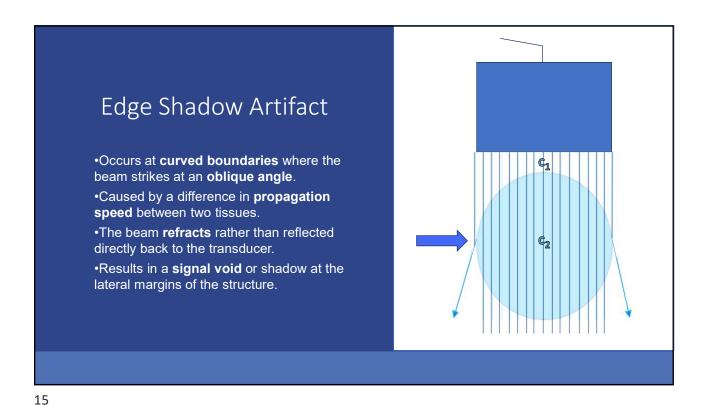
- Also known as *shadowing by refraction*.
- Occurs when an ultrasound beam strikes a rounded or curved interface.
- Refraction causes the beam to **bend along** the structure's edge.
- Most frequently seen at the fetal skull, gallbladder wall, or rounded structures.



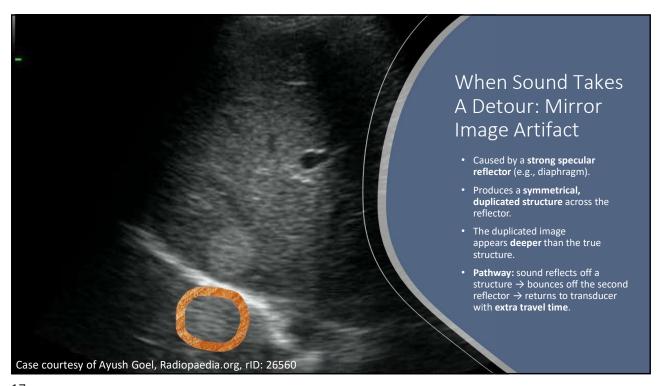
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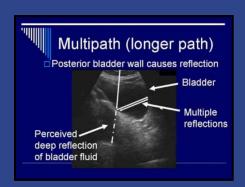
When Sound Takes A Detour: Refraction Artifact Refraction occurs when sound crosses tissue boundaries at an oblique angle and different propagation speeds. IVC The beam transmits with a bend, misplacing returning echoes laterally. Produces side-by-side duplication of structures. Artifactual duplication of the aorta due to refraction. © Nevit Dilmen, CC BY-SA 3.0 https://creativecommons.org/licenses/by-sa/3.0, via Wikimedia Commons



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When Sound Takes A Detour: Multipath Artifact

- Multipath Artifact occurs when the incident acoustic beam reflects off multiple surfaces before returning to the transducer.
- These reflections take a longer, *indirect route*, which delays their arrival.
- The machine assumes all echoes return in a straight path, so the delayed echo is placed too deep.
- * Concept: Depth error due to delayed time-of-flight from complex echo routes.



Physics of Ultrasound, Honors Ultrasound Group of The Ohio State University College of Medicine; www.youtube.com/@jchanmeister, 3:11-4:01

Speed Displacement Artifact

- **What You Need to Know:**
- Occurs when ultrasound travels through tissue with a propagation speed that deviates from the assumed soft tissue average of 1540 m/s.
- Structures may appear closer or farther than they really are.
 - Slower tissue (e.g., fat) = structure appears too deep
 Faster tissue (e.g., muscle) = structure appears too shallow
- Remember: The system assumes a uniform speed of sound. Any deviation breaks that assumption!



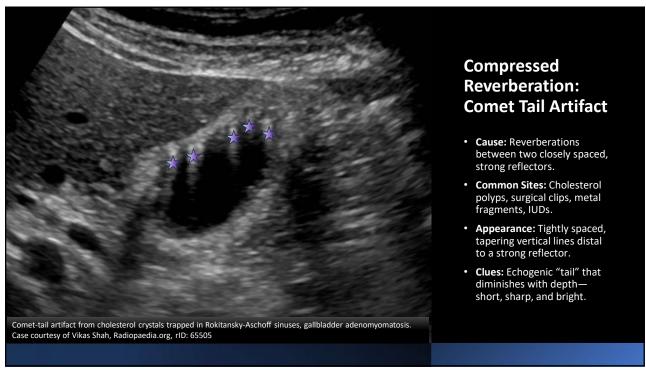
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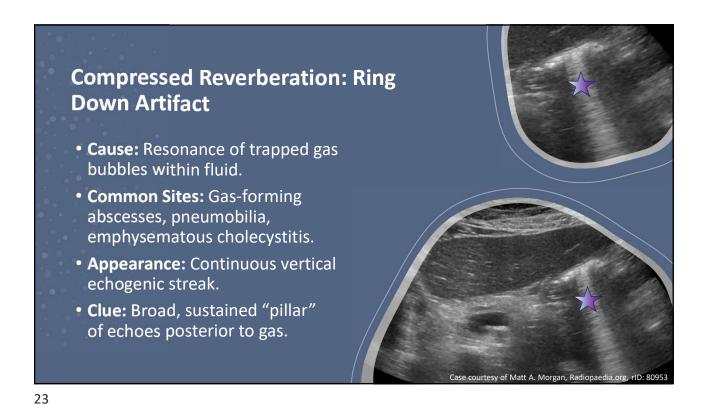


Reverberation Artifact: The Ping-Pong Effect

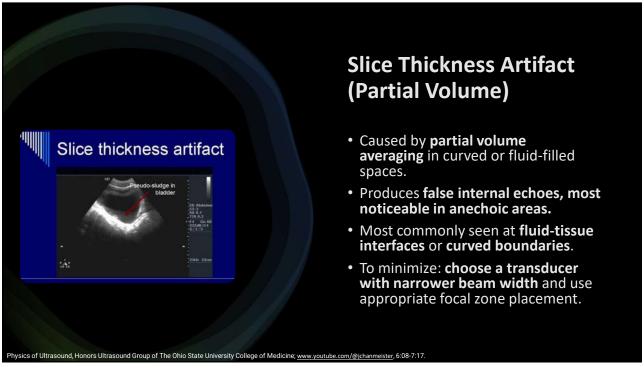
- Caused by repeated reflections between two strong, parallel reflectors.
- Produces equidistant horizontal lines decreasing in intensity.
- Seen near-field in structures like the bladder, pleura, gallbladder.
- Sound doesn't take a detour like in some of our previously reviewed artifacts—it bounces back and forth, like a ping-pong ball.

Summary Comparison: Refreshing on Items We've Covered So Far Artifact **Primary Cause Echo Error Common Appearance Distinguishing Feature** Sound bouncing Horizontal, equally Reverberation Too many echoes (depth) seen in bladder, between two strong spaced lines gallbladder, pleura Echo takes indirect Deeper copy; less Deep, misplaced or return via multiple Echo arrives late Multipath symmetrical than mirror duplicated structures surfaces Echo bounces off strong Symmetrical false liver/diaphragm or **Mirror Image** reflector (e.g. False copy across line duplicate bladder; duplications diaphragm) look real Beam bends at oblique Requires different speeds Refraction angle through speed-Echo shifted laterally Side-by-side duplication + oblique angle; e.g., change zones double aorta





Cause: Reflections from energy outside the main ultrasound beam (side lobes or beam width). Appearance: False echoes within anechoic or cystic structures. **Lobe Artifacts** Common Sites: Gallbladder, bladder, cysts—any fluid-filled Diagnostic Tip: Use TGC to lessen echo visibility from off-axis reflections, employ harmonics to suppress off-axis energy return, use proper focal zone placement. <u>Feature</u> Side Lobes **Grating Lobes** All transducers Only in array transducers Occurs in (mechanical & array) (linear, curvilinear, etc.) Beam diffraction, Improper element spacing, Cause secondary emissions particularly >½ λ Can produce false duplicate Usually low-level echoes **Artifact Severity** Fill-in of anechoic areas; May cause fill-in of more disruptive, may mimic anechoic areas real structures Apodization, focusing Suppression (splitting crystals) Example Artifact Spurious echoes Spurious or duplicate echoes Case courtesy of David McGrath, Radiopaedia.org, rID: 46955



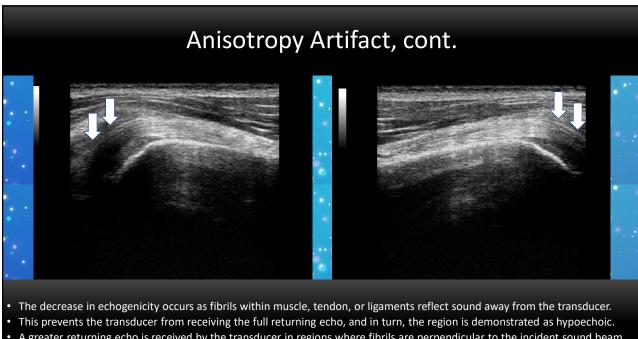
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Anisotropy Artifact

- Anisotropy occurs when the ultrasound beam strikes linear fibrous structures—such as tendons, nerves, or muscles—at a nonperpendicular angle, leading to a hypoechoic appearance.
- Most commonly seen in **musculoskeletal imaging**, it can falsely mimic pathologies like tendon tears or fluid collections.
- The artifact results from angle-dependent reflectivity; echogenicity decreases as the transducer tilts away from 90° incidence.
- Corrected by angle manipulation—using the "heel-toe" or rock-and-tilt technique to restore perpendicular insonation and eliminate this decrease in echogenicity.



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A greater returning echo is received by the transducer in regions where fibrils are perpendicular to the incident sound beam.

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Anisotropy Artifact

Anisotropy must be differentiated from hypoechoic tendinopathy.

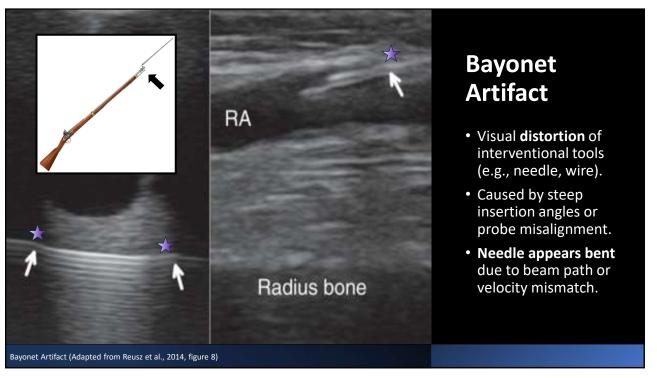
Differentiation is achieved by modifying the transducer's angle of insonation.

Anisotropy can be useful for confirming tendon position, as it is only producible in the linear tendon, while the surrounding nonlinear echogenic fat is unaffected.

This creates an increase in contrast between the tendon and surrounding tissues.

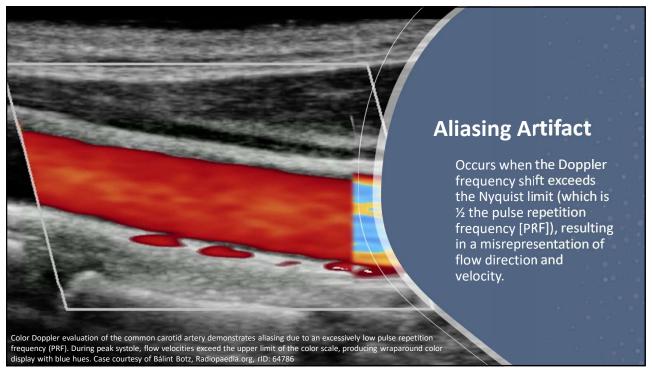
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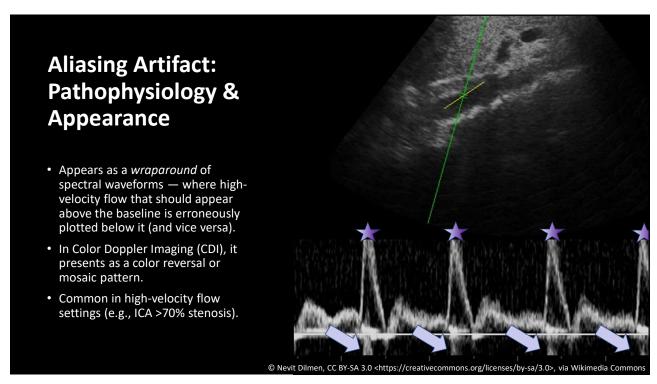
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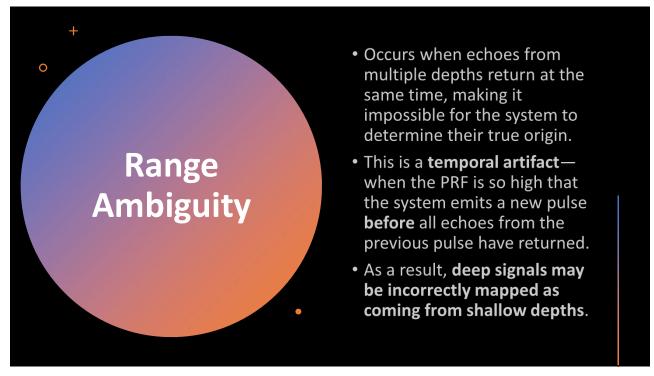
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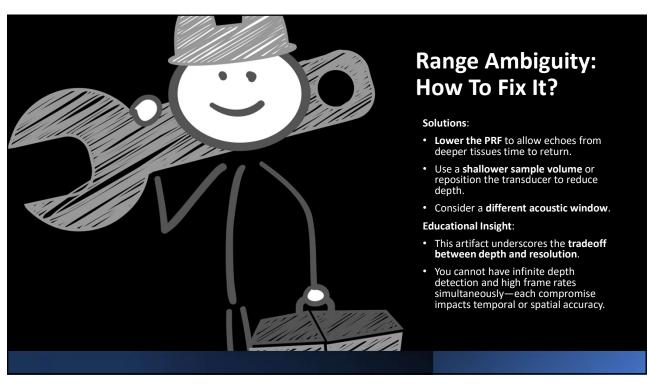


Aliasing Artifact: How To Fix It? Solutions: Increase PRF (though limited by depth). Lower the transmitted Doppler frequency. Use a shallower sample gate. Shift the baseline to display more of the waveform above/below. Switch to Continuous Wave (CW) Doppler, which can measure any velocity but sacrifices range resolution.



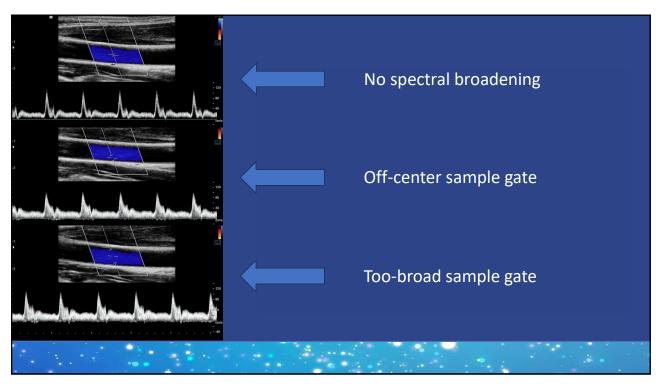
Range Ambiguity

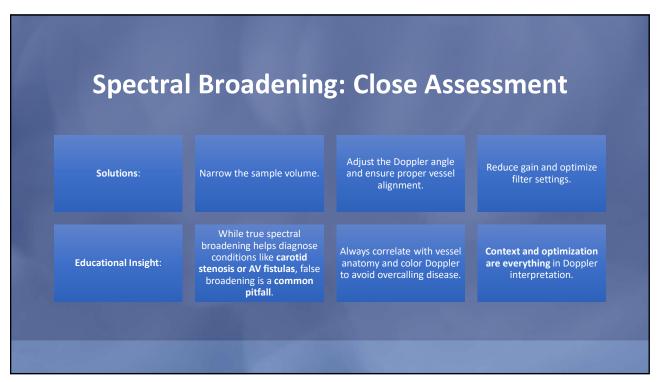
- Appearance:
 - May look like duplicated or superimposed spectral signals.
 - In spectral Doppler, this mimics turbulence or abnormal hemodynamics.
- Risk Factors:
 - High PRF to reduce aliasing (ironically trades one artifact for another).
 - Imaging deep structures (e.g., renal arteries, iliac vessels).



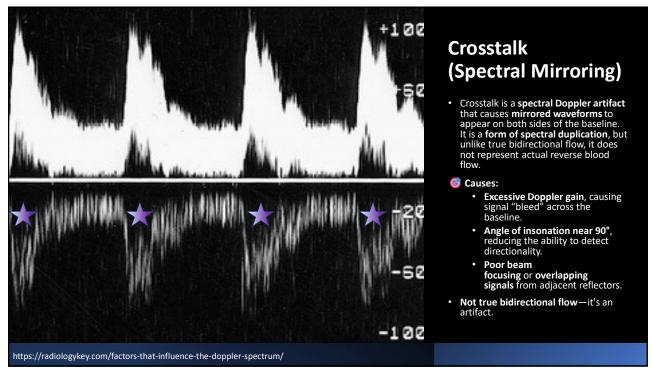
Spectral Broadening • Spectral broadening refers to the widening of the Doppler spectral envelope, indicating a range of velocities within the sample volume. True Spectral Broadening: • Represents turbulent or disturbed flow, where many velocities exist at once (e.g., post-stenotic turbulence). • Appears as a "filled-in" spectral window.

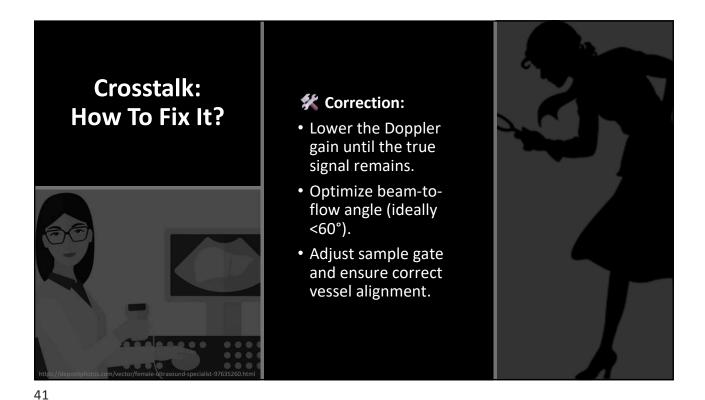
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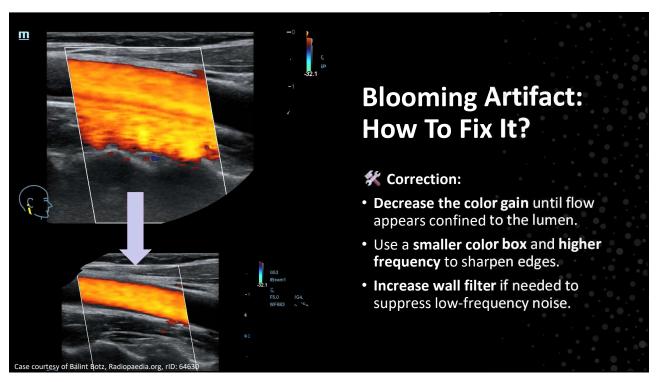


Blooming Artifact:
Color Doppler Overgain

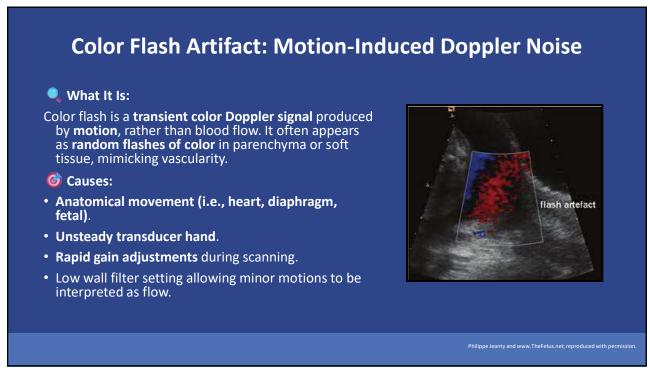
What It Is:
Blooming occurs when color Doppler signals extend beyond the boundaries of a vessel wall.

Causes:
Overgained color Doppler, resulting in signal spill.
Low wall filter settings, allowing more signal spread.

Case courtey of Bálint Botz, Radiopaedia.org, r1D: 64630



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Color Flash Artifact: Assess and Correct Increase wall filter to suppress low-frequency tissue motion. Minimize transducer motion; use a light and steady hand. Observe for persistence—real flow has continuity, while flash is sporadic and while flash is sporadic and

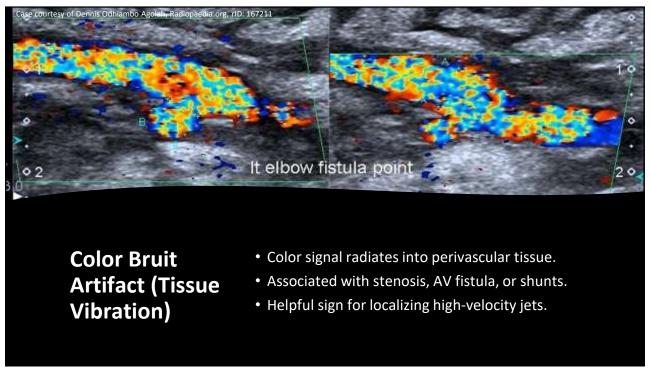
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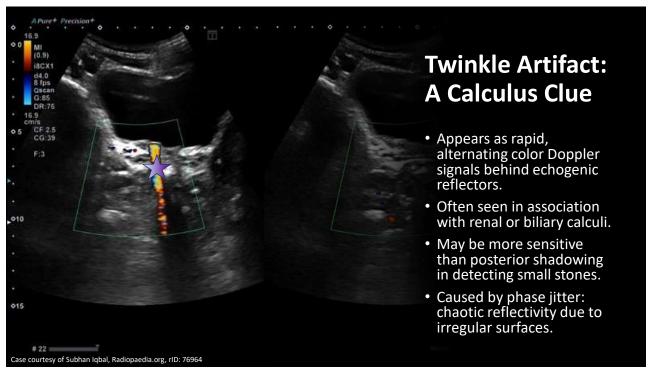
Ghosting/Clutter (Wall Motion Artifact)

motion-related.

- Ghosting Artifact (Color Doppler): Lowvelocity tissue motion (e.g., vessel wall pulsation, probe movement) appears as false color flow—often symmetrical and peripheral to real flow.
- Clutter Artifact (Spectral Doppler): Lowamplitude, non-phasic echoes appear near the baseline, simulating low-velocity blood flow.
- Common Causes: Excessive gain, low wall filter settings, patient motion, probe instability.
- How to Reduce: Increase wall filter, reduce color or Doppler gain, hold the transducer steady, avoid 90° beam-to-flow angles.

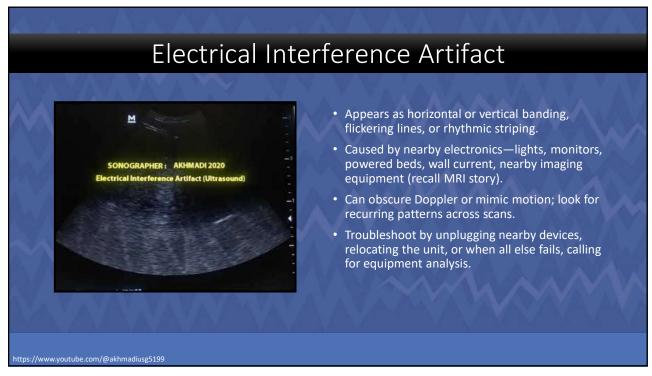


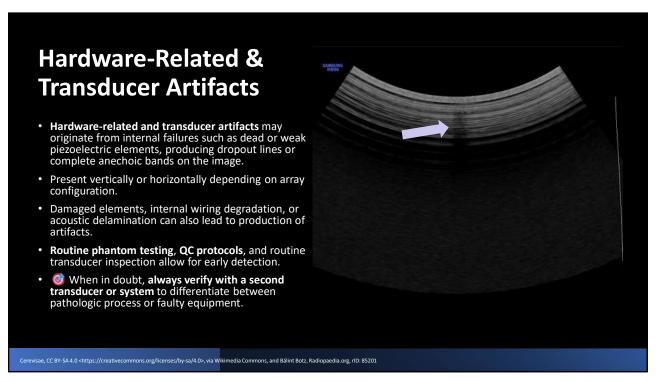
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Image Optimization

What tools are in our toolbox?

Harmonic Imaging

- Harmonic imaging leverages non-linear wave propagation, capturing echoes at higher frequencies generated within tissues.
- It reduces near-field clutter, side lobe artifacts, and reverberation to enhance contrast and border definition in technically difficult patients.
- However, harmonics may suppress low-level echoes such as sludge, debris, or microbubbles, potentially masking important subtle pathology.
- Sonographers should toggle harmonic imaging on and off when evaluating cystic and vascular structures.



Figures 4-1 and 4-2. https://radiologykey.com/tissue-harmonic-imaging-and-doppler-ultrasound-imaging/

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Spatial Compounding

- Spatial compounding acquires echoes from multiple steering angles, then integrates them into a single real-time frame.
- This reduces noise, lobe artifacts, and posterior acoustic features, like shadowing (e.g., from stones) or enhancement (e.g., behind cysts).
- Trade-off: Spatial compounding degrades temporal resolution.
- Machine-specific implementations include GE's CrossXBeam, Philips' SonoCT, and Canon's ApliPure+—often toggled in preset or "advanced imaging" menus.

Focal Zone and Gain Adjustment

- Focal zone should be placed at or just below the area of interest.
- Correct placement enhances lateral resolution, improving margin and interface clarity.
- Overall gain controls global brightness; TGC allows depth-specific finetuning for uniform brightness.
- Over-gaining can obscure pathology, while under-gaining may falsely render echocontaining structures as anechoic.



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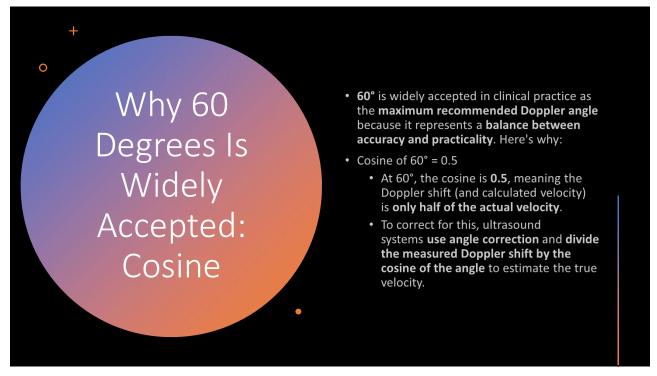


Doppler Optimization

- Adjust PRF and wall filter based on expected flow velocity and vessel type.
- Keep Doppler angle ≤ 60° to ensure velocity accuracy and avoid cosine error.
- Use a small sample gate placed in the center of the vessel and a narrow color box to improve frame rate.
- Dynamic adjustments during scanning are needed to accommodate flow variability.

Clinical Impact of Cosine Error At 0°, the cosine is 1.0, meaning 100% of the Doppler shift is detected, and The Doppler equation is: calculated velocity is accurate (not $f_D = \frac{2f_0v\cos(\theta)}{}$ always practically achievable) • At **60°**, the cosine is 0.5 — half of the ullet f_D is the Doppler shift velocity is reflected in the signal. f₀ is the transmitted frequency v is the velocity of blood flow $oldsymbol{ heta}$ is the Doppler angle • At **75°**, cosine drops to 0.26 — which causes serious underestimation of actual flow velocity.

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Why 60 Degrees Is Widely Accepted: Cosine

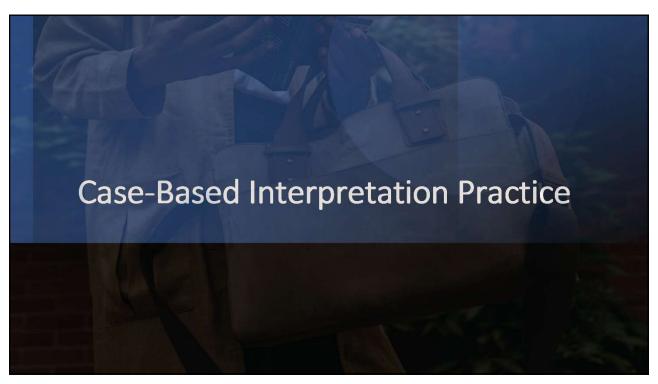
- At 60° , $\cos(60^{\circ}) = 0.5$
- The system calculates:
 - True velocity = Observed Doppler shift / 0.5
 - So the system effectively doubles the measured shift to estimate the true velocity.
- Small errors in angle correction (like misaligning 65° instead of 60°) lead to larger velocity calculation errors.
 - For example:
 - $cos(60^\circ) = 0.5$
 - $cos(70^\circ) = 0.342$
 - Just a 10° difference causes a 31% error in cosine, and therefore velocity!

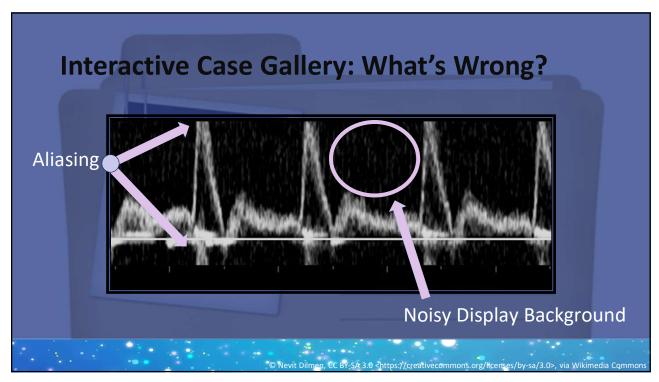
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0 Angles lower than 60° are Why 60 more accurate (cosine closer to 1.0), but often hard to Degrees Is achieve in practice due to patient anatomy and Widely transducer positioning. • 60° strikes a practical Accepted: **compromise**: relatively easy to achieve, and still yields Practicality reasonably accurate velocity estimates.

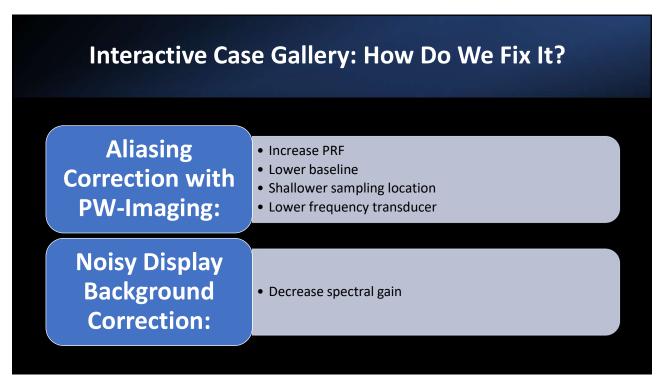
Why Not Go Beyond 60°?

- As the Doppler angle approaches 90°, cosine approaches 0, and errors become extreme.
- At 80°, for instance, $cos(80^\circ) = 0.17$ any small mistake in angle correction causes massive velocity miscalculations.
- At 90°, cos(90°) = 0, meaning no Doppler shift is recorded at all you're insonating perpendicular to flow.



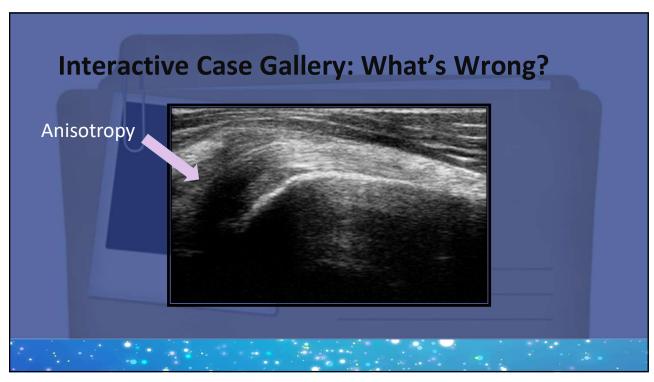


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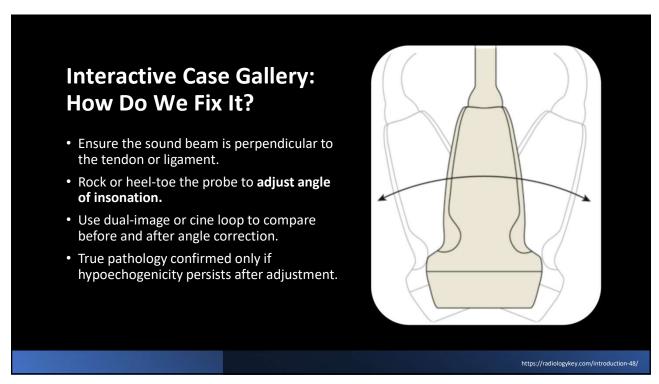


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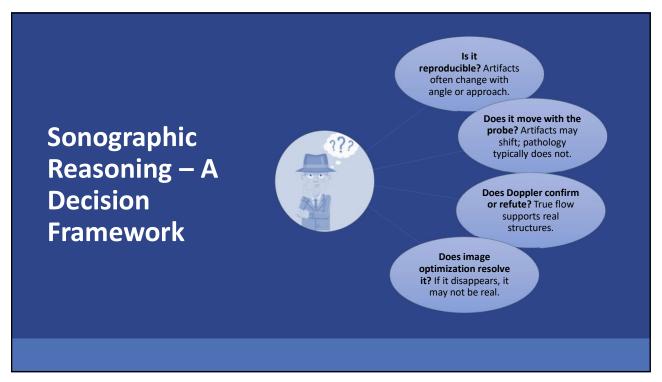


Clinical Significance & Wrap-Up

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Diagnostic Impact of Misinterpreted Artifacts

- Misread artifacts can lead to unnecessary imaging, biopsies, or surgery.
- Missed pathology may delay life-saving interventions.
- Overestimation may cause patient anxiety or overtreatment.
- Accurate interpretation ensures **appropriate**, **timely care**.



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Summary & Takeaways Artifacts can be both diagnostic allies and confounding traps. Recognize patterns and use the tools in your toolbox to assess. Confident scanning = reliable interpretation + better patient care. Let's wrap up with a Q&A session to test your knowledge!

Q&A



Which grayscale ultrasound artifact produces a symmetrical duplication of an anatomical structure across a highly reflective interface, with the duplicate image appearing deeper than the true anatomical structure?

- A. Refraction
- **B.** Reverberation
- C. Mirror Image Artifact
- **D.** Crosstalk

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Q&A



Mirror Image Artifact

Which grayscale ultrasound artifact appears as vertical echogenic bands extending posteriorly from gas collections or bubbles?

A. Comet tail
B. Ring down
C. Reverberation
D. Refraction

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Q&A



While performing spectral Doppler analysis, you notice that the waveform is symmetrically mirrored across the baseline. The insonation angle is near 90°, and the Doppler gain appears elevated. Which artifact is most likely present?

- A. Aliasing
- **B.** Mirror image artifact
- **C.** Spectral broadening
- **D.** Crosstalk

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Q&A



Crosstalk

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Thank You

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